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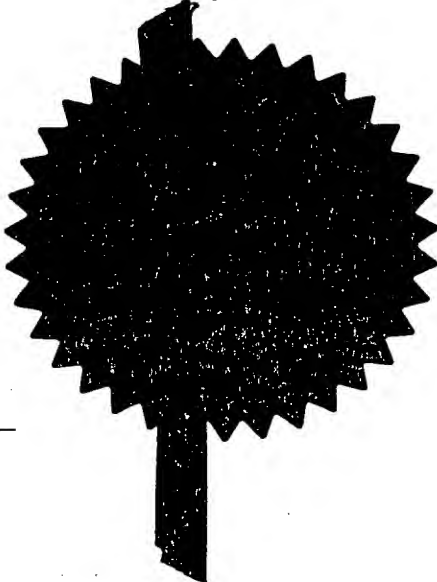
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The Patent Office

Cardiff Road  
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1. Your reference

GCN/2171GB

2. Patent application number

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9725209.2

3. Full name, address and postcode of the or of each applicant (underline all surnames)

SMITH & NEPHEW PLC  
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Patents ADP number (if you know it)

03969284001

If the applicant is a corporate body, give the country/state of its incorporation

UNITED KINGDOM

4. Title of the invention

CELL CULTURE PRODUCTS

5. Name of your agent (if you have one)

JOHN HOBBS

"Address for service" in the United Kingdom to which all correspondence should be sent (including the postcode)

SMITH & NEPHEW GROUP RESEARCH CENTRE  
CORPORATE PATENTS & TRADE MARKS DEPARTMENT  
YORK SCIENCE PARK  
HESLINGTON  
YORK YO1 5DF

Patents ADP number (if you know it)

7260854001

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Country

Priority application number  
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Number of earlier application

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Is a statement of inventorship and of right to grant of a patent required in support of this request? (Answer 'Yes' if:

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Claim(s)

Abstract

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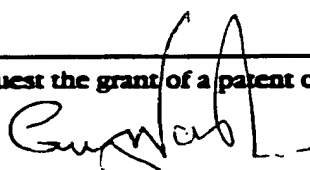
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## **CELL CULTURE PRODUCTS**

The present invention relates to the culturing of mammalian anchorage dependent cells onto a carrier substrate. More  
5 particularly, the present invention relates to wound dressings suitable for treating e.g. partial thickness wounds such as burns or skin graft donor site and to systems for the preparation of such dressings.

10 The current widely practised approach to the treatment of severe skin trauma necessitates the removal of dead tissue which might otherwise support the proliferation of pathogenic micro-organisms. However, this procedure often leaves massive open wounds which require closure and the use of autologous skin grafts  
15 is not particularly desired for a number of reasons, not least because there may be, in cases of serious burns for example, a limited supply of unaffected tissue. Cadaver skin grafts have been used to temporarily close a wound site but its limited supply and the perceived concern with cross-contamination with bacterial or viral  
20 pathogens has led to a search for alternatives.

In recent years, techniques for the *in vitro* cultivation of keratinocytes from human epidermis have been developed for culturing on epidermal sheets to cover full thickness burns. In the  
25 earliest versions of this approach, a confluent usually multilayered keratinocyte sheet was grown on tissue culture plastic *in vitro*. The cell layer would then be detached from the culture plastic using degradative enzymes, inverted and placed upon the wound. Reports on the efficiency of this approach indicate that substantial  
30 practical difficulties exist (see, for example, J Burn Care Rehab. 13, 174-180).

More recently keratinocytes have been cultured on flexible, biocompatible membranes to facilitate the transfer of cell sheets onto the wound site. See, for example, our patent application WO91/13638. Other illustrative examples of this approach include those disclosed in WO88/08448, EP 0364306, EP 0387975 and US 5266480. One difficulty with prior art approaches is that the use of membranes optimised for keratinocyte attachment thereto during the culturing phase can often inhibit the migration of the cells from the membrane onto the wound, following the application of the wound dressing. Indeed, the prior art has tended to concentrate on improving the attachment of cells to the membrane, see for example US 5558861 where the use of microbially produced cellulose is disclosed having an animal cell adhesive protein physically or chemically bonded thereto, the express aim of which is to provide a cellulose gel having an excellent adhesion to epidermal cells.

It is therefore an object of the present invention to provide a wound dressing which comprises a carrier layer that promotes the culturing of anchorage dependent cells *in vitro* yet following application to a wound, the dressing becomes substantially non-adherent to cells.

In accordance therefore, the present invention provides a wound dressing comprising a carrier layer having a wound-facing surface, said surface being non-adherent to anchorage-dependent cells and having disposed thereon a biodegradable cell anchoring layer.

The present invention also provides a system for the culturing of anchorage dependent cells, said system comprising a wound dressing as hereinbefore described together with means for

maintaining an aqueous culture medium containing cells in contact with said cell anchoring layer of said dressing, said dressing being maintained in a submerged position.

- 5           The present invention further provides a method for the treatment of wounds comprising the step applying the dressing as described herein before to a patient.

10           By the term "biodegradable cell anchoring layer" we mean a layer, capable of anchoring cells thereto, that is susceptible to degradation or breakdown following application of the dressing to the wound.

15           It is preferred that the dressing is conformable i.e the dressing will conform to changes in contours of the body portion to which the dressing is applied.

20           In preferred embodiments the carrier layer is in the form of a gel, e.g. hydrogel, a film or sheet. A film is particularly preferred. Films suitable as the carrier layer may be continuous or apertured e.g formed into a net. The film may be flat or contoured. The contours may be produced for example by embossing. Suitably contoured films may also have apertures.

25           The carrier layer may comprise a material which is inherently non-adherent to cells or alternatively the material may be surface treated e.g coated with a non-adherent to cell material, to provide a carrier layer having a non-adherent to cell wound facing surface. It is observed that when a material is non-adherent to cells, the cells  
30           when suspended in a suitable aqueous medium in contact with the non-adherent material appear rounded up and do not attach to the

material. In contrast, where a material is adherent to cells, the cells will attach to the material and "sit down". Furthermore, the cells will resist detachment when washed gently with water.

5            Useful materials that are non-adherent to cells include cross-linked cellulose derivatives. Preferred examples thereof include cross-linked hydroxyalkyl celluloses e.g. hydroxyethyl cellulose, hydroxypropyl cellulose, methyl, ethyl and methylethyl celluloses (available from Sigma Co and Aldrich). Cross-linked carboxyalkyl  
10 celluloses are also preferred e.g. carboxymethyl cellulose (CMC, available from Hercules Ltd, Lancashire, UK) cross-linked with ethylene glycol diglycidyl ether (EGDGE) or 1,4 butanediol diglycidyl ether. Other preferred materials include polyvinyl alcohol (PVA, Sigma Co) and Cell-Form™ (ICN).

15

          Alternatively a material which is adherent to cells maybe surface treated e.g by coating with a non-adherent to cell material so as to provide a carrier layer having a non-adherent to cell wound facing surface. Illustrative examples of adherent materials  
20 employed in the present invention include polymers, particularly synthetic polymers, such as those disclosed in our patent applications WO 91/13638 and WO 97/06835. Apt polymers therefore include polyhydroxyethylmethacrylic acid (polyHEMA), cross linked polyvinylalcohol (PVA), polyacrylic acid cross linked  
25 with triallylsucrose (Carbopol), polyvinylpyrrolidone, polyetherpolyesters, polyetherpolyamides, polyacrylamides and polyethylene oxide and polyurethanes. Other apt polymers include copolymers such as those containing vinyl acetate residues such as ethylene-vinyl acetate copolymers. Suitable ethylene-vinyl acetate  
30 copolymers are those containing not more than 20% vinyl acetate. A preferred material, known as EVA 538/539 contains 16% vinyl



acetate. Other suitable polymers include essentially hydrocarbon based materials such as polybutadienes, polypropylene and polystyrene. Further examples include block copolymers having hard end blocks and softer mid blocks. Apt block copolymers include styrene based rubbers such as styrene-butadiene styrene (manufactured under the trade name CARIFLEX or KRATON, Shell chemical Co). The adherent material may then be coated on the wound facing surface with phospholcholine, or silicone, polyethylene glycol or polytetrafluoroethylene (PTFE).

10

The carrier layer may comprise a material which is biodegradable or non-biodegradable following application of the dressing to the wound site. Illustrative examples of biodegradable materials include photopolymerizable hydrogels such as those taught in US 5,410,016 and sold under the trade name FOCAL (Focal Inc, USA)

The carrier layer may also comprise a backing layer disposed on a non-wound facing surface to increase the robustness of the wound dressing. Accordingly, the wound dressing may comprise a carrier layer in the form of a laminate film comprising a carrier layer described herein before having a backing layer disposed on the non wound-facing surface. The backing layer may be fabricated from materials commonly used in the manufacture of wound dressings such as polypropylene, polyurethanes, polyesters and polyethylene. Particular preferred are polyurethanes. Preferred polyurethane backing layers include **OPSITE** (Smith & Nephew). Polyurethane backing layers may be chemically modified with treatments such as plasma treatment with nitrogen, ammonia or air, Corona discharge treatment or flame treatment to increase the surface energy of the surface of the backing layer which contacts the non wound facing

30

surface. This aims to enhance the wettability of the backing layer and thereby improve the interface between the backing layer and non wound facing surface.

5           It is preferred that the carrier layer is sterilised by any suitable known methods of sterilisation. Suitable forms of sterilisation include ethylene oxide (allowing the required time for degassing), gamma-irradiation or steam sterilisation.

10           It is preferred that the carrier layer is permeable to wound exudate so as to prevent the build-up of exudate under the wound dressing which might lead to the lifting or arching of the dressing away from the wound site and therefore reducing the effective contact area of the dressing with the wound site.

15           This permeability may be achieved by rendering the carrier layer sufficiently porous to wound exudate. Such rendering is standard practice in the art. Suitably, the carrier layer is permeable to moisture vapour, oxygen and carbon dioxide. In this way a  
20           dressing when in place on the wound will provide moist conditions allowing for the cells to remain viable while the wound heals and prevent the accumulation of wound exudate.

25           The biodegradable cell anchoring layer preferably anchors the cells indirectly, e.g. through attaching to the carrier layer an animal cell adhesion protein, the protein capable of anchoring cells. According to this approach, the cell anchoring layer preferably comprises a natural or synthetic polyanion. Preferred natural  
30           polyanions include héparans, for example, heparin, heparin sulphate, fucoidin, (available from Sigma Co) syndecan, betaglycan

and perlecan. Other preferred natural polyanions include inositol phosphates e.g. inositol hexaphosphate, dextran sulphate, pentosan and mesoglycans (available from Sigma Co). A synthetic polyanion such as polyvinyl sulphate ( available from Sigma Co) may be used.

5

The polyanion is preferably cross-linked. This may be achieved by the addition of an effective amount of a cross-linking agent e.g. EGDGE. It is preferred that a polyanion is utilised due to its non-specific binding properties with respect to animal cell

10 adhesion proteins. That is, polyanions are capable of binding a large variety of animal cell adhesion proteins. As a result, the cell anchoring layer having a variety of animal cell adhesion proteins attached thereon is capable of anchoring more cells since it increases the probability that the cells will be expressing at least one

15 factor capable of being anchored to at least one type of animal cell adhesion protein. Furthermore, polyanions bind growth factors, e.g. epidermal cell growth factors for example fibroblast growth factor (FGF). Therefore, advantageously, this promotes the formation of an engraftable cell layer. A source of animal cell adhesion proteins

20 comprising a multitude of different cell adhesion proteins is preferred. Foetal calf serum (FCS) is a preferred source.

Preferably, to form the biodegradable anchoring layer, the

25 polyanion is first made up into aqueous solution and maybe either spread on or sprayed onto the non-adherent to cell layer and allowed to dry. The polyanion may then be cross-linked as described herein before.

Alternatively the cell anchoring layer may anchor the cells directly. Short specific peptides e.g. RGD, YIGSR (available from Sigma Co) may be grafted onto non-adherent to cell layer.

Alternatively, a polycationic peptide may anchor the cell  
5 directly. An example of which is polylysine (Sigma Co).

The cells of the present invention are preferably mammalian epithelial or mesenchymal cells e.g. keratinocytes or fibroblasts.  
10 Melanocytes may also be used. It is preferred for burn and chronic wounds that keratinocytes are used. Preferably the keratinocytes are autologous cells, harvested according to standard techniques of the art.

15 Alternatively, a mixture of autologous and allogenic cells could be utilised with the present invention. In particular, where the main clinical concern is rapid closure of a dermal wound, a wound dressing according to the present invention comprising e.g. 90% allogenic keratinocytes and 10% autologous keratinocytes may be  
20 provided. The aim of which is to produce rapid wound closure following the application of the dressing. Following which, the autologous cells will progressively repopulate the wound site as the allogenic cells are rejected.

25

In a further alternative embodiment, the wound dressing of the present invention may comprise a mixture of keratinocytes and fibroblasts. It has been shown that the addition of fibroblasts to keratinocyte cultures markedly increases the production of  
30 basement membrane components. Such an effect may be usefully

exploited to overcome the known weakness in the dermal-epidermal junction observed with current epidermal grafts.

5       The wound dressing of the present invention may be used in the treatment of a variety of wounds. The dressing of the invention is particularly suitable for treating partial thickness wound e.g. where the epidermis and possibly only part of the dermis is lost. Such wounds include skin graft donor sites, first or second degree burns, shallow leg ulcers or pressure sores. The dressing may also be  
10       used for full thickness wounds e.g. venous ulcers. In addition, the dressing of the present invention may find further use as part of a treatment for the chronic skin wounds that may develop following tumour excision and radiotherapy.

15       The wound dressing of the present invention may be prepared in accordance with standard cell culture techniques. The dressing may be placed in a suitable, preferably transparent, culture vessel with the cell anchoring layer face up. The vessel may be formed from suitable materials conventionally used in the manufacture of  
20       tissue culture vessels. High impact polystyrene is preferred. The dressing is then submerged in an aqueous medium comprising the cells and, if appropriate, the cell adhesion proteins. The medium utilised may be those commonly used in the field, e.g. dulbecco's modified eagle's medium (DMEM). The medium further comprises  
25       the usual nutrients, e.g. glucose, non-essential amino acids etc. Sufficient time is elapsed to allow the cells to become anchored to the cell anchoring layer and form a preferably sub-confluent layer.

30       It is preferred, however, to pretreat the carrier layer of the present invention e.g. by washing, with a solution of adhesion proteins such as FCS and then placing the dressing in a culture

vessel comprising the aqueous media which includes nutrients, O<sub>2</sub> etc. and the cells. This accelerates the attachment of the cells by providing the cells with a ready-made layer i.e. the cell anchoring layer, on which to be anchored.

5

The dressing may then be removed from the culture vessel and applied to the wound of a patient, bringing the cell layer into contact with the wound site. The dressing may then be secured to the patient and left in place on the wound. Over a period of time, the cell anchoring layer which is suitably susceptible to enzymatic breakdown by e.g. proteases and heparinase present in the wound site, will degrade or breakdown, releasing the cell layer anchored thereto into the wound site. The non-adherent to cell layer disposed on the wound facing surface discourages re-attachment of the cells to wound dressing.

10

15

If clinical concern dictates, proteases or heparinases may be added by the physician to the dressing once in place to accelerate the release of the cell layer.

20

The invention will now be illustrated by way of non-limiting examples.

#### Example 1

25

Carboxymethyl cellulose (Blanose™, Aqualon), was dissolved as a 1% aqueous solution. EGDGE (20% w/w, Aldrich) was added and the solution mixed briefly using a magnetic stirrer. The resulting mixture was allowed to stand at 37°C for 16 hours. **Opsite IV 3000** (Smith&Nephew) polyurethane film was exposed to nitrogen plasma (1 minute; 100W; Chamber pressure 0.1 to 0.2 mbar; using a PT7300 etcher) and promptly covered with a thin coat of EGDGE/CMC reaction mix (approx. 0.05ml/cm<sup>2</sup>). An aqueous

30

solution of heparin (10mg/ml; 0.1ml/cm<sup>2</sup>) was then sprayed on top of the CMC/EGDGE coating and the resulting material dried at 60 °C for 5 hours. The resulting films were then sterilised and stored dry.

- 5           The films were then immersed in Foetal Calf Serum (40%w/w, GIBCO) in phosphate buffer saline (PBS) for 16 hours at 37°C. The films were then washed twice with PBS and human keratinocytes suspended in serum free Keratinocyte basal medium (KBM) supplemented with Keratinocyte growth medium (KGM) growth  
10 additives (available from Clonetics, Walkersville, Maryland USA). Cells adhered to the film within 16 hours with a favourable level of spread and adherence after 2 days.

### Example 2

#### 15   Preparation of methyl cellulose/EGDGE/polylysine films

Carbonate buffer, pH 11, was prepared as follows:

Solution A = 10.6g Na<sub>2</sub>CO<sub>3</sub> in H<sub>2</sub>O (500ml)

Solution B = 8.4g NaHCO<sub>3</sub> in H<sub>2</sub>O (500ml)

- 20   Solution C = 330ml Solution A + 170ml Solution B adjusted to pH 11 with NaOH.

- Methyl cellulose (1g, Aldrich Chemicals) was dissolved in buffer (solution C) (100ml, pH 11; stir for 16 hours at room temperature). A  
25 hydrophilic polyurethane (PU) sheet (IV3000, Smith & Nephew) and was treated with Corona discharge to increase its hydrophilicity (2 meters/min, 0.3 kW, Aluminium trough electrode; Sherman Instruments). Methyl Cellulose solution (10g) was mixed with  
Ethylene Glycol DiGlycidyl Ether (EGDGE, 10µl) and the resulting  
30 solution spread on the polyurethane film using a spreading block to give a methyl cellulose/EGDGE film of 18/1000 inch thick. The

spread PU film was then heated (60°C, 1 hour). Polylysine in aqueous solution (1mg/10cm<sup>2</sup>, Sigma) was sprayed onto the spread PU film and dried for 2 hours at 60°C. The films were washed twice with DMEM and twice in serum-free media (Gibco).

- 5 Trypinised cells (primary human keratinocytes) were resuspended in serum-free media and added to the films.